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(54) Multi-layer drug delivery system

(57) A dispenser for use in a fluid environment which is capable of delivery of a plurality of discrete drug containing layers comprises a rigid housing (20), a fluid activated driving member (34), sets of moveable longitudinally aligned drug layers (24-32) which erode on contact with the fluid at an outlet (22) and are thus dispersed. Driving member (34) is e.g. an osmotic pump, gas generating composition etc.

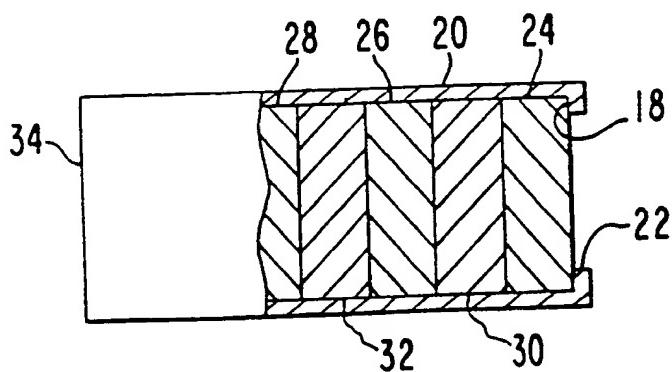


FIG. 1

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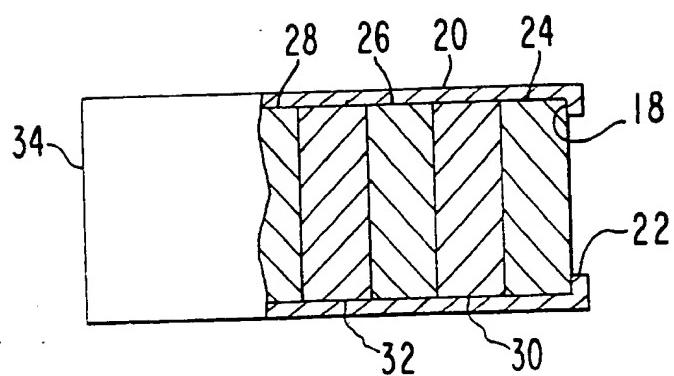


FIG. 1

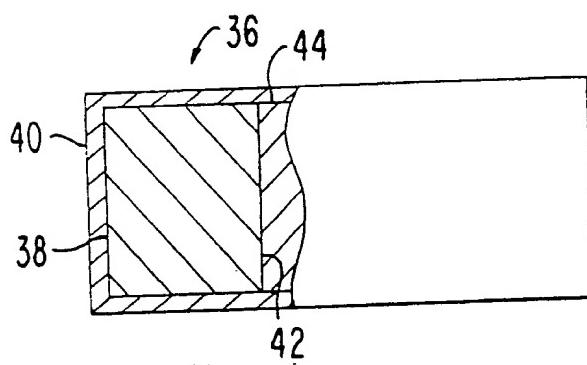


FIG. 2

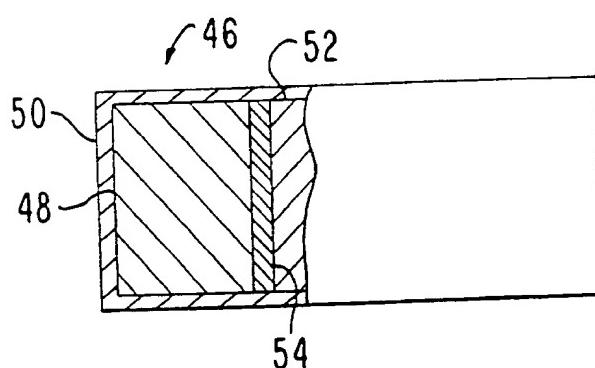


FIG. 3

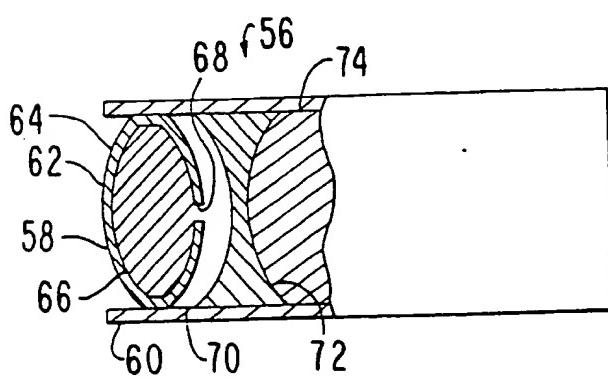


FIG. 4

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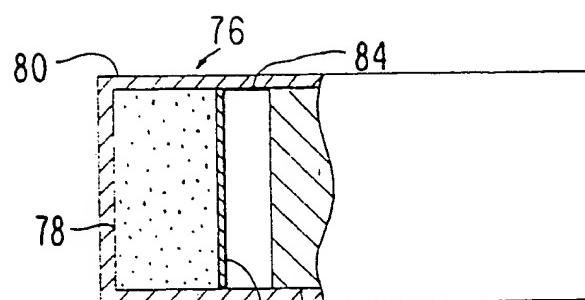


FIG. 5

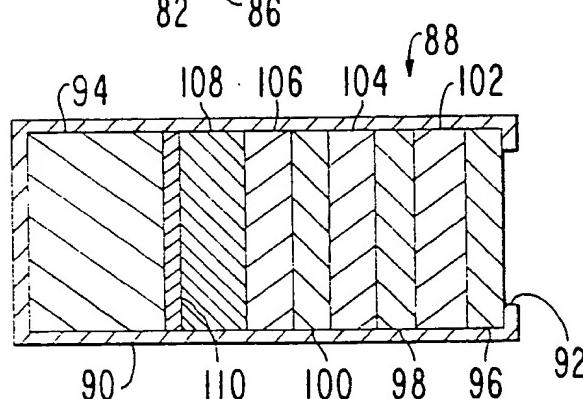


FIG. 6

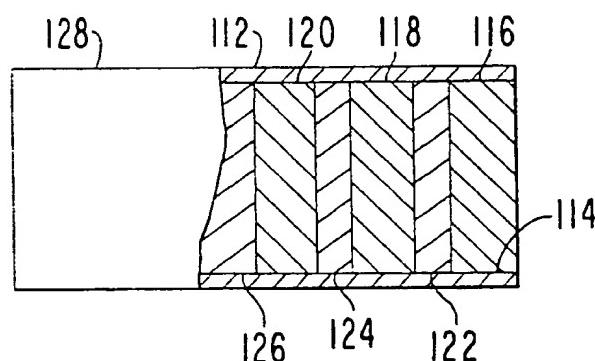
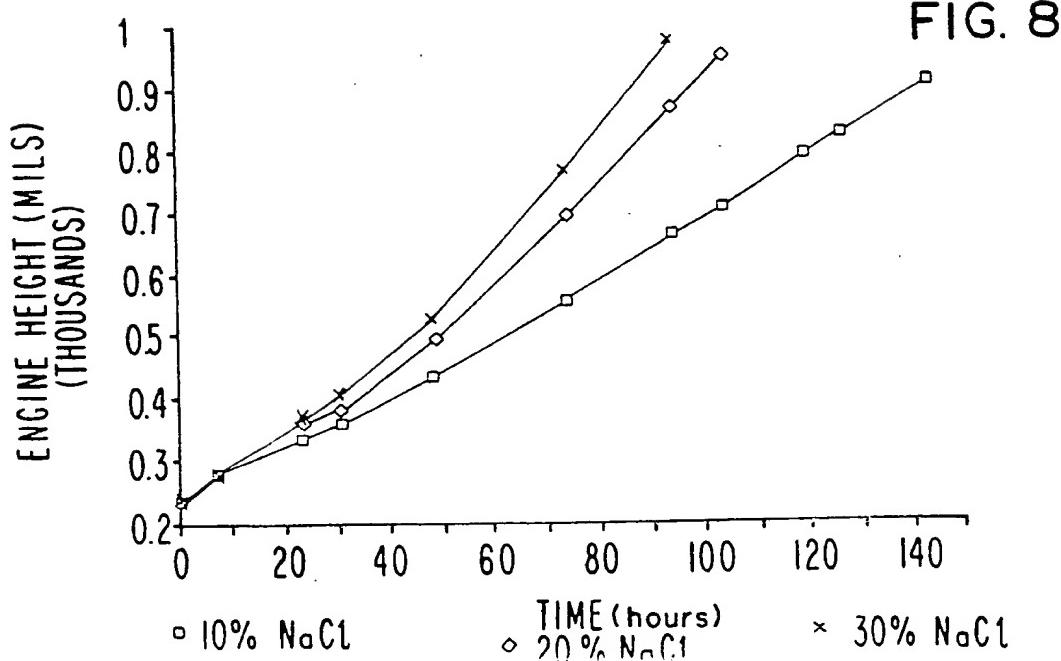


FIG. 7



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FIG. 9

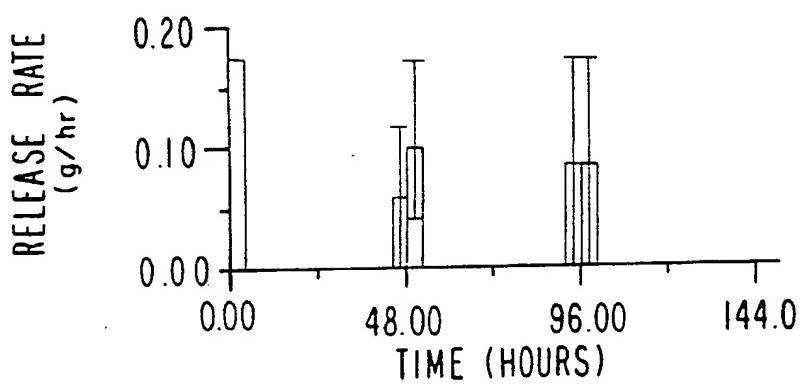
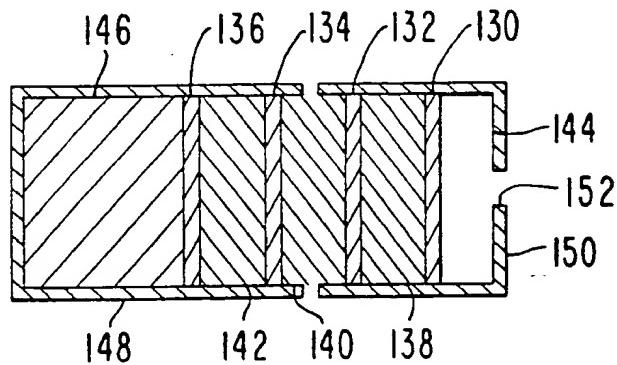


FIG. 10



MULTI-LAYER DELIVERY SYSTEM

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DESCRIPTION

This invention relates to patterned drug delivery.
5 More particularly, this invention relates to patterned drug delivery by means of a plurality of drug delivery layers. Still more particularly, but without limitation thereto, this invention relates to delivery of multi-agents orally or in other media in a
10 pre-programmed delivery profile.

The expressions "active agent" and "drug" are used interchangeably and as used therein broadly include any compound, composition of matter or mixture thereof, that can be delivered from the system to produce a beneficial and useful result. This includes pesticides, herbicides, germicides, biocides, algicides, rodenticides, fungicides, insecticides, anit-oxidants, plant growth promotors, plant growth inhibitors, preservatives, antipreservatives, disinfectants, sterilization agents, catalysts, chemical reactants, fermentation agents, foods, food supplements, nutrients, cosmetics, drugs, vitamins, sex steriliants, fertility inhibitors, fertility promotors, air purifiers, micro-organism attenuators
20 and other agents that benefit the environment of use.
25

The terms "active agent" and "drug" as used herein further includes any physiologically or pharmacologically active substance that produces a localized or systemic effect or effects in animals, including warm blooded mammals, humans and primates, avians, domestic household, sport or farm animals such as sheep, goats, cattle, horses and pigs, or is administered to laboratory animals such as mice, rats and guinea pigs, to fish, reptiles, zoo and wild animals. The active drug which can be delivered includes inorganic and organic compounds including without limitation, those materials that act upon the central nervous system such as hypnotics and sedatives, psychic energizers, tranquilizers, anticonvulsants, muscle relaxants, antiparkinson agents, analgesics, anti-inflammatory, local anesthetics, muscle contractants, anti-microbials, anti-malarials, hormonal agents including contraceptives, sympathomimetics, diuretics, anti-parasites, neoplastics, hypoglycemics, nutritional, fats, ophthalmic, electrolytes and diagnostic agents.

The term "drug layer" as used herein includes wax formulations, solid cores or tablets, with or without excipients for controlling erosion.

As used herein the expression "external fluid" includes water and other biological fluids.

Background of the Invention

The concept of patterned drug delivery covers a broad range of systems from time release capsules whose components have

coatings which erode at different rates, to controlled release rate tablets which operate by osmosis.

Despite the development of the art however, there remains a continuing need for improved methods and systems for providing controlled drug release profiles on a larger scale.

Summary of the Invention

An object of this invention is to provide sequential timing and dispensing of delivery layers containing the same or different active agents.

Another object of this invention is to provide both a novel and useful agent formulation delivery system that is self-contained, self-powered and also represents an improvement in the delivery art.

These and other objects are demonstrated by the present invention wherein a drug dispenser for use in a fluid containing environment comprises a rigid housing, a plurality of movable drug layers filling a portion of the housing, a fluid activated driving member for displacing the drug layers filling the remainder of the housing and a drug outlet means.

Brief Description of the Drawings

The invention will be described in further detail with reference to the accompanying drawings wherein:

Figure 1 is a partial cross-sectional view of the dispenser of this invention, illustrating one embodiment of the dispensing configuration;

Figure 2 is a partial cross-sectional view of one embodiment of the driving member for the dispenser of this invention, utilizing a hydrophilic expandable member;

5 Figure 3 is a partial cross-sectional view of a second embodiment of the driving member for the dispenser of this invention, utilizing an osmotically effective solute;

Figure 4 is a partial cross-sectional view of another embodiment of the driving member for the dispenser of this invention, utilizing an elementary osmotic pump;

10 Figure 5 is a partial cross-sectional view of another embodiment of the driving member for the dispenser of this invention, utilizing a gas generating composition;

15 Figure 6 is a cross-sectional view of one embodiment of the dispenser of this invention capable of delivering a plurality of discrete drug layers alternating with drug/wax formulations, and having a hydrogel driving member;

Figure 7 is a partial cross-sectional view of the dispenser of this invention, illustrating another embodiment of the dispensing configuration;

20 Figure 8 is a graph depicting the expansion of the driving member in relation to the NaCl content;

Figure 9 is a graph of the drug release rate profile of the dispenser of Fig. 7; and

25 Figure 10 is a cross-sectional view of another embodiment of the dispenser of this invention capable of providing a plurality of drug pulses.

Description of the Preferred Embodiment

This invention can provide a variety of drug delivery profiles including, but not limited to, pulsed delivery of a single drug or drug formulation, pulsed delivery of a sequence of different drugs or drug formulations, pulsed delivery of one drug or drug formulation superimposed on continuous delivery of a different drug or drug formulation, and simultaneous continuous delivery of several drugs or drug formulations.

The drug dispenser of this invention is designed to deliver a drug or drug formulation by displacement of a plurality of discrete longitudinally aligned individual drug layers by the linear expansion of a fluid activated driving member. It is comprised of a dispensing component and a driving component, representative embodiments of which are disclosed herein. Figures 1, 6, 7 and 10 illustrate various embodiments of the dispensing component suitable for use in the dispenser of this invention. These configurations can be combined with various embodiments of the driving component, representative embodiments of which are illustrated in Figures 2-5.

The dispensing and driving component designs are for use in a fluid-containing environment and are merely exemplary of the numerous embodiments suitable for use in this invention. The portion of the housing adjacent to the dispenser component is of a material which can be either semipermeable or impermeable to the passage of external fluid. Typical impermeable materials include polyethylene, polyethylene terephthalate (Mylar), plasticized polyvinyl chloride, metal-foil polyethylene

laminates, neoprene rubber, natural gum rubber, and Pliofilm (rubber hydrochloride). These materials are additionally flexible, insoluble and chemically compatible with the active agent contained in the layers positioned therein, and, in the instance of providing a drug or like depot within the body of a living organism, are biologically inert, non-irritating to body tissues and non-allergenic. Additional suitable materials include polystyrene, polypropylene, polyvinyl chloride, reinforced epoxy resin, polymethylmethacrylate, etc., sheet metal (e.g., aluminum, copper, steel, etc.), galvanized pipe, or styrene/acrylonitrile copolymer. Again, for drug depot applications, the same are advantageously biologically inert, non-irritating to body tissue and non-allergenic. Suitable semipermeable materials include all cellulosic polymers such as cellulose acetates, ethylcellulose, methylcellulose, cellulose acetate butyrate, cellulose acetate propionate, etc. or blends of an impermeable material and a hydrophilic polymer or a low molecular weight water soluble enhancer to render the material semipermeable.

Many other materials including those which are biologically acceptable are suitable for fabrication of the impermeable portion of the housing. While this portion has previously been described as being insoluble under the conditions and in the environment of intended use, it is also within the scope of the invention that such materials be insoluble only during the period of said intended use; thereafter dissolving away in the environment of the device. Thus, a dispenser is here contemplated which is unaffected by its environment, solubility-wise, at the

situs of use, or which is only slightly soluble during the period of intended use, such that once its active agent content has been removed it will then dissolve or erode away leaving no objectionable residue or empty container at the said situs of
5 use.

The portion of the housing adjacent to the driving component may be of the same material. However, several of the driving component designs operate by the imbibition of external fluid.
10 For those particular embodiments, the portion of the housing adjacent thereto, must be semipermeable and allow passage of external fluid. Suitable materials will be described with reference to the specific driving member embodiments.

The dispensing component shown in Figure 1 is comprised of a rigid housing member 20. Housing 20 is also designed with an outlet means, exit port 22. A plurality of movable discrete layers 24, 26, 28, 30 and 32, are aligned within the housing 20. This configuration is merely illustrative and the dispenser may have numerous drug layers in excess of the number shown in Fig. 1.

20 The drug layers can erode or disintegrate and can be in the form of a wax formulation, solid core or tablet. The layers can immediately dissolve upon exposure to fluid or they may erode slowly with or without the presence of excipients for controlling erosion. The layers can be designed in a multitude of ways to provide a specific drug delivery profile. Layers which immediately dissolve provide pulsed drug delivery while layers which erode provide continuous delivery for the duration of the layer.

As stated above, one embodiment consists of layers which slowly disintegrate upon contact with the external fluid. These layers may contain a biologically acceptable solid surfactant which is capable of slow dispersion in the environmental fluid.

5 In another embodiment, the layers may be susceptible to erosion upon contact with the external fluid and contain a fluid insoluble wax such as stearic acid, paraffin wax or beeswax, and a non-ionic surfactant such as ethoxylated alcohols and polyether, both being biologically acceptable. In still another

10 embodiment, the layers may be effervescent and provide drug delivery in a finely dispersed form. This is accomplished by the addition of a solid basic compound capable of evolving carbon dioxide in the presence of an acid in the environment of use. Suitable basic compounds are disclosed in U.S.Pat.No. 4,265,874,

15 incorporated herein by reference.

The driving member 34 operates to displace the layers towards the exit port 22. As the layers come into contact with the exit and are exposed to the external fluid, they begin to erode in a controlled or semi-controlled fashion. The exit port 22 is fashioned with a lip 18 which acts to keep the layers intact within the housing 20 as it erodes. This provides continuous delivery of drug until layer 24 is completely eroded. Once layer 24 is completely eroded, linear displacement pushes layer 30 through the housing 20 so that it comes into contact with exit 22.

In one embodiment, layers 24, 26, 28, 30 and 32 contain different drugs or drug formulations. In another embodiment,

layers 24, 26 and 28 may contain the same or different drugs or drug formulations and layers 30 and 32 can be comprised of an inert hydrophobic gel such as petrolatum. This would provide an "off" period during which time no drug is being delivered.

5 Additionally, the layers may be effervescent to shorten the pulse time.

For ruminal systems, an important criteria is that the system remain in the rumen of an animal over a prolonged period of time. This is accomplished by placement of a density element 10 within the dispenser. The housing 20 itself, may be the density element. Alternately, unit 28 can be a density element, placed so as to remain within the housing 20 after all of the drug layers have eroded.

The density element suitable for use in the dispenser of this invention must be dense enough to retain the dispenser in the rumen-reticular sac of a ruminant. The presence of a density element allows the dispenser to remain in the rumen over a prolonged period of time rather than letting it pass into the alimentary tract and be eliminated therefrom. As the dispenser remains in the rumen, a beneficial agent can be delivered to the ruminant at a controlled rate over an extended period of time. Generally, a density element will have a density of from about 15 0.8 to 8, or higher, with the density in a presently preferred embodiment exhibiting a specific gravity of from about 2.2 to 20 7.6. For the ruminants cattle and sheep, it is presently preferred that the density element exhibit a density such that 25 there is a resulting dispenser density of about 3. Materials that have a density that can be used for forming a suitable density

element include iron, iron shot, iron shot coated with iron oxide, iron shot magnesium alloy, steel, stainless steel, copper oxide, a mixture of cobalt oxide and iron powder, and the like.

Exemplary of drugs that are soluble or very soluble in water and can be delivered by the dispenser systems of this invention include prochlorperazine edisylate, ferrous sulfate, aminocaproic acid, potassium chloride, mecamylamine hydrochloride, procainamide hydrochloride, amphetamine sulfate, benzphetamine hydrochloride, isoproterenol sulfate, methamphetamine hydrochloride, phenmetrazine hydrochloride, bethanechol chloride, metacholine chloride, pilocarpine hydrochloride, atropine sulfate, methscopolamine bromide, isopropamide iodide, tridihexethyl chloride, phenformin hydrochloride, methylphenidate hydrochloride, and mixtures thereof.

Exemplary of agents that have limited solubility or are very slightly soluble, or insoluble in water and biological fluids that can be delivered by the dispenser systems of this invention include diphenidol, meclizine hydrochloride, prochlorperazine maleate, thiethylperazine maleate, anisindione, diphenadione, erythrityl tetranitrate, digoxin, isofluorophate, reserpine, azetazolamide, methazolamide, bendroflumethiazide, chlorpropamide, tolazamide, chlormadinone acetate, phenaglycodol, allopurinol, aluminum aspirin, methotrexate, acetyl sulfisoxazole, erythromycin, and mixtures thereof, steroids including corticosteroids such as hydrocortisone, hydrocorticosterone acetate, cortisone acetate and triamcinolone, anhydrogens such as methyltestosterone, estrogenic steroids such as

17 β -estradiol, ethinyl estradiol, ethinyl estradiol 3-methyl ether and estradiol, progestational steroids such as prednisolone, 17 α -hydroxy-progesterone acetate, 19-norprogesterone, norethindrone, progesterone, norethynodrel, and the like.

The drug can also be in the various chemical and physical forms such as uncharged molecules, molecular complexes, pharmacologically acceptable acid addition and base addition salts such as hydrochlorides, hydrobromides, sulfate, laurylate, palmitate, phosphate, nitrate, borate, acetate, maleate, tartrate, oleate and salicylate. For acidic drugs, salts of metals, amines or organic cations, for example quaternary ammonium can be used. Derivatives of drugs such as esters, ethers and amides can be used alone or mixed with other drugs. Also, a drug which is water insoluble can be used in a form that on its release from the dispenser, is converted by enzymes, hydrolyzed by body pH or other metabolic processes to the original form, or to a biologically active form.

The dispensing configuration of Figures 1, 6, 7 and 10, can be combined with any of the driving members illustrated in Figures 2-5 to provide a tailored drug delivery system.

Figure 2 illustrates a driving member system 36 utilizing an expandable driving member 38 comprised of an external fluid insoluble, external fluid swellable composition. Member 38 is encased in housing 40 which is a semipermeable membrane substantially permeable to the passage of an external fluid and substantially impermeable to the passage of any ingredients contained in member 38. The driving member 38 is positioned

adjacent to one of the drug layers at interface 42.

External fluid is imbibed through the housing 40 by the expandable hydrophilic member 38 in a tendency toward osmotic equilibrium, to continuously swell and expand member 38. Member 38 expands while maintaining an intact immiscible boundary at interface 42, defined by the surface of drug layer 44 and expandable member 38.

Expandable member 38 has a shape that corresponds to internal shape of housing 40 and is preferably made from a hydrogel composition. The hydrogel composition is noncross-linked or optionally cross-linked and it possesses osmotic properties, such as the ability to imbibe an external fluid through semipermeable housing 40, and exhibit an osmotic pressure gradient across semipermeable housing 40 against a fluid outside the dispenser system. The materials used for forming the swellable, expandable member 38 are polymeric materials neat, and polymeric materials blended with osmotic agents that interact with water or a biological fluid, absorb the fluid and swell or expand to an equilibrium state. The polymer exhibits the ability to retain a significant fraction of imbibed fluid in the polymer molecular structure. The polymers in a preferred embodiment are gel polymers that can swell or expand to a very high degree, usually exhibiting a 2 to 50 fold volume increase. The swellable, hydrophilic polymers, also known as osmopolymers, can be noncross-linked or lightly cross-linked. The cross-links can be covalent, ionic or hydrogen bonds with the polymer possessing the ability to swell in the presence of fluid, and when cross-linked

it will not dissolve in the fluid. The polymer can be of plant, animal, or synthetic origin. Polymeric materials useful for the present purpose include poly(hydroxyalkyl methacrylate) having a molecular weight of from 5,000 to 5,000,000;

5 poly(vinylpyrrolidone) having a molecular weight of from 10,000 to 360,000; anionic and cationic hydrogels; poly(electrolyte) complexes; poly(vinyl alcohol) having a low acetate residual; a swellable mixture of agar and carboxymethyl cellulose; a swellable composition comprising methyl cellulose mixed with a sparingly cross-linked agar; a water swellable copolymer produced by a dispersion of finely divided copolymer of maleic anhydride with styrene, ethylene, propylene, or isobutylene; water swellable polymer of N-vinyl lactams; swellable sodium salts of carboxy methyl cellulose; and the like.

15 Other gelable, fluid imbibing and retaining polymers useful for forming the hydrophilic, expandable driving member 38 include pectin having a molecular weight ranging from 30,000 to 300,000; polysaccharides such as agar, acacia, karaya, tragacanth, algin and guar; Carbopol® acidic carboxy polymer and its salt derivatives; polyacrylamides; water swellable indene maleic anhydride polymers; Good-rite® polyacrylic acid having a molecular weight of 80,000 to 200,000; Polyox® polyethylene oxide polymers having a molecular weight of 100,000 to 5,000,000; starch graft copolymers; Aqua-Keep® acrylate polymers with water absorbability of about 400 times its original weight; diesters of polyglucan; a mixture of cross-linked polyvinyl alcohol and poly(N-vinyl-2-pyrrolidone); poly(ethylene glycol) having a molecular weight of 4,000 to 100,000; and the like. In a

preferred embodiment, the expandable member 38 is formed from polymers and polymeric compositions that are thermoformable.

5 Representative polymers possessing hydrophilic properties are known in U.S.Pat.Nos. 3,865,108, 4,002,173, 4,207,893, 4,220,152, 4,327,725, 4,350,271, all of which are incorporated herein by reference and in Scott et al, "Handbook of Common Polymers", CRC Press, Cleveland, Ohio (1971).

10 The osmotically effective compound that can be blended homogeneously or heterogeneously with the swellable polymer, to form a driving member, are the osmotically effective solutes that are soluble in fluid imbibed into the swellable polymer, and exhibit an osmotic pressure gradient across the semipermeable housing 40 against an external fluid. Osmotically effective compounds are known also as osmagents. Osmotically effective 15 osmagents useful for the present purpose include magnesium sulfate, magnesium chloride, sodium chloride, lithium chloride, potassium sulfate, sodium sulfate, mannitol, urea, sorbitol, inositol, sucrose, glucose and the like. The osmotic pressure in atmospheres, atm, of the osmagents suitable for the invention will be greater than zero atm, generally from 8 atm up to 500 20 atm, or higher.

25 Representative materials for forming the semipermeable housing include without limitation, semipermeable homopolymers, semipermeable copolymers, and the like. In one embodiment typical materials include cellulose esters, cellulose monoesters, cellulose diesters, cellulose triesters, cellulose ethers, and cellulose ester-ethers, mixtures thereof, and the like. These

cellulose polymers have a degree of substitution, D.S., on their anhydroglucose unit form greater than 0 up to 3 inclusive. By "degree of substitution" is meant the average number of hydroxyl groups originally present on the anhydroglucose unit that are replaced by a substituting group, or converted into another group. The anhydroglucose unit can be partially or completely substituted with groups such as acyl, alkanoyl, aroyl, alkyl, alkenyl, alkoxy, halogen, carboalkyl, alkylcarbamate, alkylcarbonate, alkylsulfonate, alkylsulfamate, and like semipermeable polymer forming groups.

The semipermeable materials typically include a member selected from the group consisting of cellulose acylate, cellulose diacylate, cellulose triacylate, cellulose acetate, cellulose diacetate, cellulose triacetate, mono-, di- and tri-cellulose alkanylates, mono-, di- and tri-alkenylates, mono-, di- and tri-aroylates, and the like. Exemplary polymers including cellulose acetate having a D.S. of 1.8 to 2.3 and an acetyl content of 32 to 39.9%; cellulose diacetate having a D.S. of 1 to 2 and an acetyl content of 21 to 35%; cellulose triacetate having a D.S. of 2 to 3 and an acetyl content of 34 to 44.8% and the like. More specific cellulosic polymers include cellulose propionate having a D.S. of 1.8 and a propionyl content of 38.5%; cellulose acetate propionate having an acetyl content of 1.5 to 7% and a propionyl content of 39 to 42%; cellulose acetate propionate having an acetyl content of 2.5 to 3%, an average propionyl content of 39.2 to 45% and a hydroxyl content of 2.8 to 5.4%; cellulose acetate butyrate having a D.S. of 1.8, and acetyl content of 13 to 15%, and a butyryl content of 34 to 39%;

cellulose acetate butyrate having an acetyl content of 2 to 29.5%, a butyryl content of 17 to 53%, and a hydroxyl content of 0.5 to 4.7%; cellulose triacylates having a D.S. of 2.9 to 3 such as cellulose trivalerate, cellulose trilaurate, cellulose 5 tripalmitate, cellulose trioctanoate, and cellulose tripropionate; cellulose diesters having a D.S. of 2.2 to 2.6 such as cellulose disuccinate, cellulose dipalmitate, cellulose dioctanoate, cellulose dicarpylate; cellulose propionate morpholinobutyrate; cellulose acetate butyrate; cellulose acetate phthalate; and the like; mixed cellulose esters such as cellulose acetate valerate, cellulose acetate succinate, cellulose propionate succinate, cellulose acetate octanoate, cellulose valerate palmitate, cellulose acetate heptonate, and the like. Semipermeable polymers are known in U.S.Pat.No. 4,077,407, and 10 they can be made by procedures described in "Encyclopedia of Polymer Science and Technology", Vol. 3, pages 325-354, 15 Interscience Publishers, Inc., New York, (1964).

Additional semipermeable polymers include cellulose acetaldehyde; dimethyl cellulose acetate; cellulose acetate ethylcarbamate; cellulose acetate methylcarbamate; cellulose 20 dimethylaminoacetate; a cellulose composition comprising cellulose acetate and hydroxypropyl methylcellulose; a composition comprising cellulose acetate and cellulose acetate butyrate; a cellulose composition comprising cellulose acetate butyrate and hydroxypropyl methylcellulose; semipermeable polyamides; semipermeable polyurethanes; semipermeable 25 polysulfanes; semipermeable sulfonated polystyrenes; crosslinked,

selectively semipermeable polymers formed by the coprecipitation of a polyanion and a polycation as disclosed in U.S.Pat.Nos. 3,173,876, 3,276,586, 3,541,005, 3,541,006 and 3,546,142, all of which are incorporated herein by reference; selectively semipermeable silicon rubbers; semipermeable polymers as disclosed by Loeb and Sourirajan in U.S.Pat.No. 3,133,132, incorporated herein by reference; semipermeable polystyrene derivatives; semipermeable (polysodiumstyrenesulfonate); semipermeable poly(vinylbenzyltrimethyl) ammonium chloride; semipermeable polymers exhibiting a fluid permeability of 10^{-1} to 10^{-7} (cc.mil/cm²hr-atm) expressed as per atmosphere of hydrostatic or osmotic pressure difference across a semipermeable wall. The polymers are known to the art in U.S.Pat.Nos. 3,845,770, 3,916,899 and 4,160,020, all of which are incorporated herein by reference; and in J.R. Scott and W.J. Roff, "Handbook of Common Polymers", CRC Press, Cleveland, Ohio (1971).

Other materials that can be used to form the semipermeable housing for imparting flexibility and elongation properties to the wall, for making the housing less to non-brittle and to render tear strength include phthalate plasticizers such as dibenzyl phthalate, dihexyl phthalate, butyl octyl phthalate, straight chain phthalates of six to eleven carbons, diisononyl phthalate, diisodecyl phthalate, and the like. The plasticizers include nonphthalates such as citric acid esters, triacetin, dioctyl azelate, epoxidized tallate, triisooctyl trimellitate, triisononyl trimellitate, sucrose acetate isobutyrate, epoxidized soybean oil, and the like. The amount of plasticizer in the housing when incorporated therein, is about 0.01 to 20% by

weight, or higher.

Figure 3 illustrates a driving member 46 utilizing an osmotically effective solute. The osmotically effective solute is in solution 48 which is retained within a rigid housing 50 comprised of a semipermeable membrane substantially permeable to the passage of an external fluid and substantially impermeable to the passage of the osmotically effective solute contained in solution 48. The solution 48 is separated from the drug layers 52 for example, by means of a flexible membrane 54.

The ability of driving member 46 to displace the drug layers, 52 for example, housed within a dispenser depends upon the osmotic pressure generated by the solution 48 of the osmotically effective solute confined within housing 50. This solution exhibits an osmotic pressure gradient against fluid in the environment into which the dispenser is placed, and is preferably a saturated aqueous salt solution. To maintain the solution saturated and therefore to achieve a constant osmotic pressure throughout operation of the dispenser, the housing containing the solution also contains excess solute in solid form. Various osmotically effective solutes can be used. These include magnesium sulfate, magnesium chloride, sodium chloride, potassium sulfate, sodium carbonate, sodium sulfite, sodium sulfate, sodium bicarbonate, potassium acid phthalate, calcium bicarbonate, potassium acid phosphate, raffinose, tartaric acid, succinic acid, calcium succinate, calcium lactate and magnesium succinate. The excess solid solute can be in the form of dispersed particles or preferably in the form of a pellet. The

solution can initially be a solution of the same or of an osmotically effective solute different than the solid excess solute.

Figure 4 illustrates a driving member 56 which is similar in 5 operation to that of Fig. 3. An elementary osmotic pump 58 such as that disclosed in U.S.Pat.No. 3,845,770, incorporated herein by reference, is held rigidly in place in the impermeable housing 60 being exposed to the environment at surface 62. External fluid is imbibed through the semipermeable wall 64 by the osmotically 10 effective solute 66 contained within the pump 58. As the osmotic pressure within the pump 58 increases, solution (external fluid and osmotic solute) is forced through the orifice 68 into chamber 70, thereby exerting pressure on piston 72 which subsequently moves through the housing 60 to dispense the drug layers 74 15 contained therein. In order for this driving member to be operable, the wall of the housing 60 immediately surrounding the pump 58, must be impermeable to the passage of fluid so that external fluid does not enter chamber 70. Therefore, use of driving member 56 mandates that the housing be at least in part 20 of an impermeable composition.

Figure 5 illustrates a driving member 76 which operates by means of a gas generating composition 78. Housing 80 is made of a semipermeable material which is substantially impermeable to the passage of gas generating composition 78, has a low permeability 25 to the passage of an internally generated gas and is substantially permeable to the passage of an external fluid. Membrane 82 is made of a semipermeable material which is substantially impermeable to the passage of gas generating

composition 78 and substantially permeable to the passage of a generated gas. Its main function is to keep the gas generating composition 78 apart from the drug layers contained in the dispenser.

5 In operation, external fluid is imbibed through housing 80 to continuously wet and dissolve the gas generating composition 78, causing it to react and produce a large volume of gas. This gas expands and passes through membrane 82, filling the space 84. This action correspondingly causes pressure to be exerted on the
10 drug layer 86 which thereby pushes this and the other layers contained therein, through the housing 80.

Gas generating composition 78 consists essentially of a dry compound or an anhydrous mixture of compounds that when intimately contacted by an external fluid that enters the housing 80, generates a gas that exerts a pressure to drive the dispensing system. The composition 78 comprises a preferably solid acidic material, and a preferably solid basic material that dissolve and react in the presence of fluid that enters the housing 80. This composition may be in powder, crystalline,
15 granular or layered form. Alternately, the gas generating composition may be present homogeneously or heterogeneously dispersed within a matrix. The matrix is a polymer permeable to the passage of external fluid and permeable to the passage of the generated gas. The rate of gas generated in this embodiment is governed by the rate of fluid passage through the polymer coupled
20 with the rate of fluid passage through the housing. Suitable materials are disclosed in Theeuwes, U.S.Pat.No. 4,203,441,
25

incorporated herein by reference.

Figure 6 illustrates an embodiment which combines the delivery methods of erosion and osmotic bursting, and is explained in detail by the following example.

5

EXAMPLE I

The dispenser 88 shown in Fig. 6 is especially suited for use as a ruminal bolus for the treatment of liver flukes, endoparasites and ectoparasites. Different drugs are need to treat endo- and ectoparasites than are needed to treat liver flukes. Additionally, treatment for parasites must be continuous while that for liver flukes may be pulsed, i.e. timed to the appropriate stage in the life cycle. Therefore, separate treatments and dosage forms are required to treat these conditions.

The housing 90 is injection molded, having an exit port 92 at one end and a driving member 94 at the opposite end. The housing is filled with a plurality of discrete drug layers 96, 98 and 100. These layers are separated by drug wax formulation layers 102, 104 and 106. The housing also contains a density element 108 which may be monolithic, multilayered or particulate in nature. The driving member 94 may be any of the embodiments disclosed herein. Especially suitable is the osmotic system of Fig. 3 using a NaCl suspension.

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The drug layers 96, 98 and 100 are for the treatment of liver flukes. Suitable drugs include without limitation, bithionol sulfoxide, oxyclozanide, clioxanide, niclofolan, nitroxinil, rafoxanide, benzimidazole and diamfenetide. These

units osmotically burst upon exiting from the exit port 92 and therefore provide for immediate release of the drug, which will continue to be delivered for about 24 hours. The drug wax formulation layers 102, 104 and 106 are for the treatment of endoparasites and ectoparasites. A suitable formulation comprises about 12-18 weight percent ivermectin suspended in wax.

The driving member 94 is designed to allow the dispenser 88 to operate in a linear fashion. In operation, the driving member 94 imbibes external fluid through the semipermeable portion of housing 90. The NaCl suspension 94 expands and exerts pressure on flexible membrane 110 which correspondingly begins to exert pressure on element 108. Thus, the dispensing movement begins.

First, drug layer 96 which is positioned adjacent to exit port 92, is forced out of the dispenser 88 and bursts, thereby providing the environment with a pulse of drug for treatment of liver flukes. The bursting of drug layer 96 and the continuous operation of the driving member 94 linearly displace the ivermectin wax formulation 102 slowly through the exit port 92 to provide constant plasma levels of ivermectin.

This is followed by bursting of drug layer 98 and so forth until the dispenser 88 is depleted of all drug layers and wax formulation layers. The pulses of drug for the treatment of liver flukes will not interfere with the constant plasma concentrations of ivermectin since ivermectin has a half life of 3-3.5 days. An important parameter is the duration of the ivermectin layers. Each layer needs to last 21-30 days for effective treatment of endo- and ectoparasites, and must be designed accordingly.

The dispensing configuration shown in Figure 7 illustrates yet another embodiment of the invention. This configuration is comprised of a rigid housing 112 designed with an outlet means, exit port 114. A plurality of moveable discrete layers 116, 118, 5 120, 122, 124 and 126, are aligned within the housing 112. The six layers shown are merely illustrative and the actual system may have layers in excess of the number shown.

Drug layers 116, 118 and 120 are of a different composition from layers 122, 124 and 126. Drug layers 116, 118 and 120 are 10 hydrophilic in nature and are solid at storage conditions. The drug can be mixed with an osmotic agent or solute, such as those described above with reference to Figure 3. When the drug layer 116 comes into contact with the external fluid, it immediately dissolves, thereby delivering the drug contained therein, in a 15 pulsed manner. Drug/osmotic agent layer 116 is separated from drug/osmotic agent layer 118 by a solid or semisolid hydrophobic layer 122 which is immiscible with the drug/osmotic agent layers and which slowly erodes upon contact with the environment.

Layers 122, 124 and 126 may contain the same drug or a 20 different drug than the drug/osmotic agent layers 116, 118 and 120. The slow erosion process would provide continuous drug delivery for a set time period. Alternately, layers 122, 124 and 126, may not contain any drug and therefore would provide an "off" period for the system, during which no drug would be 25 delivered.

Instead of containing an osmotic agent, drug layers 116, 118 and 120 can be comprised of a drug and a thermo-responsive composition. In this manner, these layers would exhibit solid-

like properties at room temperature of 21°C, and within a few centigrade degrees thereof. Likewise, these layers would have a melting point that approximates mammalian body temperatures of 37° C, and within a few centigrade degrees thereof. The term "thermo-responsive" as used for the purpose of this invention in a preferred embodiment denotes the physical-chemical property of a composition agent carrier to exhibit solid, or solid-like properties at temperatures up to 31°C, and become fluid, semi-solid or viscous when disturbed by heat at temperatures from 31 C, usually in the range of 31°C to 45°C. Suitable materials are disclosed in U.S.Pat.No. 4,595,583 incorporated herein by reference. In this embodiment, layers 166, 168 and 170 would still be a solid or semisolid composition which is immiscible with the drug/thermo-responsive composition layers.

In operation, the dispenser of Fig. 7 can deliver pulses of drug alternating with continuous delivery of drug or alternating with "off" periods, during which time no drug is delivered, depending on whether or not the erodible layers 122, 124 and 126 contain drug.

The driving member 128 operates to linearly displace the layers towards the exit port 114. As drug layer 116 comes into contact with the exit 114 it is fluid either because it contains an osmotic agent which has formed a solution with the external fluid or because it contains a heat sensitive agent which is fluid due to the temperature of the environment of use. Drug layer 116 rapidly disintegrates when it reaches the exit 114. Next is layer 122 which is held intact within the housing 112, as

it slowly erodes. Depending on whether or not drug is contained in layer 122, erosion may provide continuous drug delivery or an "off" period. Once layer 122 is completely eroded, layer 118 is exposed and so forth until the system is depleted of layers.

5 The usefulness of the dispenser of Figure 7 as a pulsatile multi-layer delivery system is best illustrated with reference to the following example.

EXAMPLE II

10 The dispenser of Fig. 7 is especially suited for control of helminth infections in ruminants, cattle in particular. A first set of drug layers, 116, 118 and 120 are comprised of 85 weight percent Hapadex® (Schering-Plough Corporation), an anthelmintic agent for cattle, and 15 weight percent Ac-Di-Sol (brand name of croscarmellose sodium, FMC Corporation), a disintegrating agent.

15 The alternating or second set of layers 122, 124 and 126 are comprised of 80 weight percent Fischer Wax (a microfine micronized hard wax), 15 weight percent high molecular weight hydroxy propyl methyl cellulose (mol. wt. about 300,000) and 5 weight percent low molecular weight hydroxy propyl methyl cellulose (mol. wt. about 7000).

20 The driving member 128 is like that of Figure 2 and is an osmotic layer comprised of a mixture of a high molecular weight sodium carboxy methyl cellulose and sodium chloride. By proper adjustment of the NaCl content, the expansion of the osmotic layer (driving member 128) can likewise be adjusted. Figure 8 provides expansion (engine height) versus time data for varied NaCl content compositions: 10, 20 and 30 weight percent. Linear

expansion is obtainable with a 10% NaCl content. Increasing growth is attainable by increasing the NaCl content to 30%, as is evidenced by Fig. 8.

Figure 9 illustrates the release rate profile attainable 5 with the dispenser of Fig. 7. When drug layer 116 is delivered, a pulse of drug is initially delivered at $t = 0$ hours. This is followed by the slow erosion (about 2 days in duration) of non-drug containing layer 122, whereupon drug layer 118 is exposed and delivers a second drug pulse at $t = 48$ hours. Once again, 10 this is followed by an "off" period as non-drug containing layer 124 slowly erodes, thereby exposing drug layer 120 which delivers another drug pulse at $t = 96$ hours, and so forth, until the dispenser is depleted of drug and non-drug containing layers.

Figure 10 illustrates another embodiment of the dispenser 15 which provides "off" periods during which no drug is delivered. Delivery programs having an on and off cycle normally require a large dispenser volume. The embodiment of Fig. 10 allows reduction of this large volume requirement by incorporating a gas generator, alone or in combination with an osmotic agent, into 20 the drug layers 130, 132, 134 and 136.

The drug layers are contained in a two part housing unit and are separated by non-osmotically active spacers or placebo layers 138, 140 and 142. The housing is also designed with a volume expansion chamber 144 and a driving member 146. The housing has a 25 first rigid or semi-rigid portion 148 having a low permeability ($k_1\pi_1$) and a second portion or closure 150 having a high permeability ($k_2\pi_2$), where k is the permeability coefficient defined as cc of fluid/hr-cm², and π is the osmotic pressure.

In operation, the presence of a gas generator, with or without an osmotic agent, in the drug layers operates to effect its discharge as a pulse of drug delivered when the layer comes into contact with the "window" (closure 150) of highly permeable membrane in the flow path of the drug layer, said flow path being through a volume expansion chamber 144. Suitable gas generators are disclosed above with reference to Fig. 5.

The driving member 146 is that of Fig. 3, an osmotic agent. Member 146 provides low flux. When drug layer 130 for instance, contacts the volume expansion chamber 144, the gas generator and any osmotic agent contained therein gives the layer with $k_2\pi_2 \gg k_1\pi_1$, which blows out the drug layer and the drug is dispensed to the environment through exit 152.

In an alternate embodiment, spacers 138, 140 and 142 are osmotically active. Both the driving member 146 and these spacers are comprised of a salt or sugar having low osmotic activity and work together to provide a low flux drive. As noted above, when drug layer 130 contacts the high permeability closure 150, the drug is blown out.

The drug delivery program provided by the dispenser of Fig. 10 involves a series of drug pulses separated by a delay or an "off" period. The drug pulse is dependent upon the drug/gas generator/osmotic agent layer contacting the high k_n volume expansion chamber. The delay, on the other hand, is dependent upon the low flux drive provided by member 146.

The amount of drug incorporated in the layers of the dispenser of this invention varies widely depending upon the

particular drug, the desired therapeutic effect, and the time span for which it takes the drug to be released. Since a variety of sizes and compositions are intended to provide complete dosage regimes for therapy for a variety of maladies, there is no
5 critical upper limit on the amount of drug incorporated into the layers of the dispenser. The lower limit too will depend upon the activity of the drug and the time span of release from the layers. Thus, it is not practical to define a range for the therapeutically effective amount of drug to be released by the
10 individual layers, or by the dispenser as a whole.

This invention has been described in detail with particular reference to certain preferred embodiments thereof, but it will be understood that variations and modifications can be effected within the spirit and scope of the invention.

CLAIMS

1. A drug dispenser for use in a fluid-containing environment comprising in combination:

5 a rigid housing;

a fluid activated driving member filling a portion of the space within said housing and being in contact with the housing;

a first set of drug layers;

10 a second set of layers alternating with said first set of drug layers both sets of layers longitudinally aligned and contained within said housing; and

15 an outlet means in said housing that communicates with the layers.

2. A dispenser as claimed in claim 1 wherein said first set of layers deliver drug to the environment by bursting upon contact with said outlet means.

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3. A dispenser as claimed in claim 1 or claim 2 wherein said first set of layers contain a drug selected from bithionol, sulfoxide, oxy clozanide, clioxanide, niclofolan, nitroxinil, rafloxanide, benzimidazole and diamfenetide.

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4. A dispenser as claimed in any preceding claim wherein said second set of layers deliver drug to the environment by erosion.
- 5 5. A dispenser as claimed in any preceding claim wherein said second set of layers contain ivermectin suspended in wax.
- 10 6. A dispenser as claimed in any preceding claim which further comprises a density element.
7. A dispenser as claimed in any preceding claim wherein said first set of layers are comprised of a hydrophilic drug composition.
- 15 8. A dispenser as claimed in any preceding claim wherein said second set of layers are comprised of a hydrophobic composition.
- 20 9. A dispenser as claimed in claim 7 or claim 8 wherein said hydrophilic drug composition is comprised of a drug together with an osmotic agent and/or a heat sensitive agent.

10. A dispenser as claimed in claim 8 wherein said hydrophobic composition further comprises a drug.

11. A dispenser as claimed in any preceding claim
5 which further comprises a volume expansion chamber.

12. A dispenser as claimed in claim 11 wherein said first set of layers comprises a drug and a gas generator.

10
13. A dispenser as claimed in claim 12 wherein said layers further comprise an osmotic agent.

14. A dispenser as claimed in any preceding claim
15 wherein said second set of layers are non-osmotically active.

15. A dispenser as claimed in any one of claims 1
to 13 wherein said second set of layers are
20 osmotically active.

16. A dispenser as claimed in claim 1 and substantially as herein described with reference to and as illustrated in the accompanying drawings.

